

SPECIFICATION

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[METHOD AND APPARATUS FOR SOFT TISSUE ENHANCEMENT]

Cross Reference to Related Applications

This application is a continuation of co-pending U.S. Patent Application Serial No. 09/141,460 filed August 27, 1998 entitled "Vacuum Dome With Supporting Rim And Rim Cushion," which is a continuation of U.S. Patent Application Serial No. 08/698,941 filed August 16, 1996 entitled "Vacuum Dome With Supporting Rim And Rim Cushion" (now abandoned), which is a continuation-in-part of U.S. Patent Application Serial No. 08/516,623 filed August 18, 1995 entitled "Method And Apparatus For Soft Tissue Enlargement With Balanced Force Appliance" (now U.S. Patent 5,676,634), which is a continuation-in-part of U.S. Patent Application Serial No. 08/504,640 filed July 20, 1995 entitled "Method And Apparatus For Soft Tissue Enlargement By Distractive Force" (now U.S. Patent 5,695,445), which is a continuation of U.S. Patent Application Serial No. 08/220,186 filed March 30, 1994 entitled "Method And Apparatus For Soft Tissue Enlargement" (now U.S. Patent 5,536,233).

Background and Summary of the Invention

[0001] There are numerous instances where persons desire enlargement of the soft tissues in their bodies. One such instance is for the replacement of one or both breasts amputated during a mastectomy in order to restore physiological symmetry and psychological well-being. Other instances are for correction of natural abnormalities such as dimpling. Still other instances are for augmentation of physical attributes to improve cosmetics and self-esteem. These latter soft tissue enlargements are principally directed to breast enlargement in females and penis enlargement in males.

[0002] Prosthetic implants have been developed for insertion below the skin. However, the severity of the potential complications including scarring, implant rupture, capsular contracture, necrosis and implant migration as well as the recent adverse publicity thereof have significantly reduced the desirability of these implants. Thus, there is a societal need for other means to obtain soft tissue enlargement.

- [0003] Some soft tissue enlargements occur naturally. For instance, during pregnancy, the skin over a woman's abdominal region enlarges approximately nine times its previous area to accommodate the fetus without a proportional decrease in skin thickness. In other words, the abdominal skin tissue actually enlarges and does not merely stretch during pregnancy. Similarly, the skin will expand to accommodate any growth under the skin.
- [0004] In the past, plastic surgeons have used this phenomenon to their advantage to expand skin in order to accommodate prosthetic implants. To conduct this procedure, the surgeon inserts a balloon beneath the skin in the area where additional skin is desired. By progressively expanding the balloon, the skin first stretches and eventually actually grows to accommodate the increased volume underneath it. When the desired amount of skin is formed, the balloon is deflated and removed, and the implant is inserted into the cavity left by the balloon. Similar methods have been used by native African tribes to enlarge lips, nostrils, and earlobes.
- [0005] Other surgical techniques have used tissue expansion to achieve other types of soft tissue growth. For instance, balloons have been successfully expanded underneath nerves, veins, tendons, and the like to thereby elongate these tissues to repair damage and alleviate various abnormalities.
- [0006] A more advanced surgical method is known as callotasis or limb lengthening. This method comprises cutting the bone about its periphery at the location where lengthening is desired, leaving the tissues inside and around the bone intact. Brackets are attached to the bone on each side of the separation, and the bone segments are slowly pulled away from one another while remaining integral over a period of several months. Not only does this cause the mended bone to be longer, but also the soft tissue surrounding the bone actually grows to accommodate the increased limb length. Similar methods have been used by African native tribes to lengthen necks for cosmetic purposes.
- [0007] Each of these above-mentioned apparatuses and methods requires an invasive surgical technique to accomplish the soft tissue expansion. Invasive techniques increase the likelihood of the complications associated with the procedure including those mentioned above with respect to implant surgery. In addition, the expense of surgery precludes many persons from having their abnormalities corrected or physical attributes enhanced.
- [0008] Other soft tissue enlargement techniques have been developed which use other mechanisms to cause the enlargement. For instance, an instrument and technique have been developed for the non-surgical correction of inverted nipples due to short lactiferous ducts. The instrument is comprised of a cup having an internal volume shaped like that of the final desired nipple. The user places the cup over the inverted

nipple, pumps the air out of the cup with a syringe and adjusts the vacuum within the cup using a check valve to just below the threshold of discomfort. Thus attached, the device puts the lactiferous ducts in tension and extends them sufficiently after two to three months of wear at 8-12 hours per day.

[0009] Although this device is sufficient for its intended purpose, it is not suitable for general soft tissue enlargement. Laceration and contusion can occur if too strong of a suction is applied to soft tissue. As the pressure within the inverted nipple instrument is not regulated, contusion or laceration can occur. When a vacuum is developed within the cup of the instrument, an equal and opposite force is applied to the patient about the rim of the cup. Excessive contact forces against the patient can cause ulceration, laceration, and contusions. As the contact forces are not regulated in the nipple instrument, these further complications also can occur. In addition, general soft tissue enlargement is not feasible with the instrument due to the size and shape of the cup.

[0010] Another prior art device is disclosed in U.S. Patent No. 936,434 as a device for enlarging a woman's breasts. This device included a pair of cups for placement on the breasts and a pump for exhausting the air from between the cups and breasts. However, this patent provides no teaching as to the pressures to be used, the potential danger to the skin tissues, or any suggestions as to how the device is to be retained in place during use. Apparently, the device is used in a clinical setting and is not suitable for long term wear such as for 8-10 hours. As the patent suggests that the vacuum acts to cause the veins and arteries to engorge, thereby nourishing the breasts, it is clear that the patentee is suggesting that the breast tissue actually expands through this expansion of blood vessels alone. This patent has been the subject of ridicule by at least one medical authority. See "An Anthology Of Plastic Surgery" edited by Harry Hayes, Jr., M.D., Section 6, "Quackery and Nostrums" pub. 1986 by Aspen Publishers, Rockville, Maryland.

[0011] Another prior art device although notorious is worthy of note. This device is commonly referred to as a penis pump and is sold primarily as a novelty as its long-term enlargement efficacy has never been proven and is in fact universally disclaimed by its distributors. The device is comprised of a cylinder having one open end into which the penis is inserted and a pump attached to it such that a vacuum can be created within the cylinder. Not only does this device have the same drawbacks as the nipple instrument with respect to potential complications, but also it is unlikely that sufficient vacuum can be maintained by the device to cause any notable long-term soft tissue enlargement. Further, this device is apparently designed to accomplish two tasks unrelated to enlargement. First, the device is used for stimulation and sexual gratification. Second, the device is used to promote erection by drawing blood into the penis.

area of the dome, thereby creating a greater contact pressure which is still within acceptable limits. Still another approach which may very well provide a therapeutic effect would be to cycle the vacuum in the dome such that it is applied for periods of time at elevated levels and relaxed levels so that the rim might also have a cross-sectional area less than the normal area of the dome, but yet avoid creating any tissue necrosis. The cycling of the vacuum pressure in the dome could be readily achieved in an automatic manner by appropriately programming the vacuum pump and regulator. Therefore, the invention should be understood as being limited only by the current medical understanding of the causative effects of pressure sores and other tissue damage by an applied pressure or vacuum.

[0015] It is well recognized in the medical literature that decubitus ulcers are caused by unrelieved external pressure that occludes blood flow and results in tissue necrosis. In recognition of this fact, these ulcers are called pressure sores. The average capillary pressure in human skin is around 15-20 mmHg. E.M. Landis, Micro-Injection Studies of Capillary Blood Pressure in Human Skin, 15 Heart 209-228, (1930). For convenience, 20 mmHg will be used to describe this pressure throughout the remainder of this description. However, it should be understood that pressures below 20 mmHg may also be used without departing from the scope of this invention and that these lower pressures may provide additional margins in preventing damage to tissues. Therefore, the local application of an external pressure up to 20 mmHg will not collapse capillaries adjacent the location of the applied pressure and thus will not disturb the circulation. Therefore, local application of contact pressures less than or equal to 20 mmHg are well tolerated for prolonged periods of time. This tolerance has been confirmed by the inventor through use of a prototype which did not cause adverse effects after many hours of continuous use as long as the pressure under the rim remained below or around 20 mmHg.

[0016] Pressures greater than 20 mmHg will occlude the capillaries and stop tissue perfusion. Tissues can tolerate short periods of ischemia, but if the pressure is continuous and perfusion is not restored within a relatively short period of time, tissue damage will ensue. "The time factor is thus more important than pressure intensity". A pressure of 100 mmHg will lead to pathologic changes after only two hours. T. Hussain, An Experimental Study of Some Pressure Effects on Tissues, with Reference to the Bed-Sore Problem, 66 J. Path. Bact. 347-358, (1953).

[0017] The experimental results of additional investigators can be used to develop a safe time-pressure curve above which tissue damage will ensue. For instance, 20 mmHg is well tolerated for prolonged periods of time, but 40 mmHg will lead to tissue injury if the pressure is not relieved for 13 hours. The injury is more severe if the pressure is 60 mmHg, and even greater injury will result with a pressure of 100 mmHg after shorter periods of time. O. Lindan, Etiology of Decubitus Ulcers: An Experimental

Study, 42 Arch. Phys. Med. Rehab. 774-783, (1961). Similarly, a pressure of 70 mmHg, if unrelieved, will lead to pathologic changes after 2 hours. However, if the pressure is intermittent, applied 5 minutes on, and 5 minutes off, there is no pathologic tissue changes. M. Kosiak, Etiology of Decubitus Ulcers, 42 Arch. Phys. Med. Rehab. 19-29, (1961).

[0018] These findings are consistent with the clinical testing of the prototype of the breast device. It was found that a continuous pressure under the rim of 40 mmHg could be tolerated for only one hour by healthy volunteers. After one hour, the volunteers started to complain of pain which is the warning sign of impending tissue damage. Higher pressures led to pain under the rim after even shorter periods of time. Lower pressures around 30 mmHg led to pain after 4 hours. However, if the pressure is allowed to cycle, that is if it is dropped down to 0-20 mmHg to allow the tissues to temporarily reperfuse for a few minutes, higher peak pressures can be tolerated. The higher the peak pressures, the shorter they are tolerated and the longer the low pressure part of the cycle needs to be to allow the tissues to recuperate.

[0019] Therefore, pressures under the rim greater than 20 mmHg can only be tolerated if there is a means to continuously cycle the pressure peaks on and off allowing for tissue re-perfusion during the off periods. The higher the peaks, the shorter the pressures are tolerated and the longer the period of low pressure recuperation needs to be.

[0020] From the above experimental animal data and human study, the inventor concludes that 20 mmHg is the highest pressure that can be safely tolerated under the rim on a prolonged basis. Higher pressures can only be applied intermittently, and then cycled down to less than 20 mmHg.

[0021] The method of use is comprised of the steps of attaching the dome to the location of desired enlargement, and creating a vacuum within the dome. In the continuous application method in which the vacuum is applied at pressures that can be withstood continuously, the vacuum should be maintained for a minimum of eight hours per day and results should be sufficient after several months.

[0022] As indicated by the summary of the medical literature given above, a vacuum dome may also be used in alternative methods in keeping within the scope of the inventor's concept. For example, the device might have a rim cross-sectional area substantially less than the normal area of the dome and be used in either of two methods. In a first method, a somewhat lower vacuum pressure may be induced in the dome such that the opposing contact pressure under the rim may be maintained at bearable pressures for extended periods of time and yet provide a therapeutic effect. Alternatively, the vacuum in the dome may be regulated in a routine which provides somewhat higher vacuum pressures in the dome for shortened periods of time

separated by periods of lower vacuum pressures to allow tissue reperfusion. In other words, alternating cycles of high vacuum, tissue reperfusion, high vacuum, tissue reperfusion, etc., may achieve a therapeutic effect in enlarging the soft tissues. With either of these methods, the rim may have a cross-sectional area substantially less than the normal area of the dome.

[0023] In an alternate embodiment, the dome may include a flexible sheet attached about the rim and spanning the dome. The sheet may be applied to the desired soft tissue with an adhesive, and the vacuum may be applied between the dome and the sheet to introduce a tensile force to the surface of the soft tissue so as to pull the soft tissue away from the body. The adhesive may comprise typical adhesives or glues, as well as, sticky gels or sheets of double-sided adhesive tapes. Further, the adhesive may be an adhesive substance embedded in the sheet or in the rim of the dome.

[0024] In addition to the embodiments already discussed, the inventor has conceived of additional embodiments which further utilize the vacuum dome. One such embodiment is especially useful in the healing or reconstruction of amputation stumps. Whether the amputation is exemplified by an acute open wound (e.g. fingertip amputations) or an extremity amputation stump that tends to break down because of a deficiency in soft tissue padding, the growing of soft tissue may be especially advantageous in healing these wounds and adding tissue padding to what might otherwise become a chronic wound particularly susceptible to infection. In this application, the vacuum dome is supported around the amputation stump, much as taught in the inventor's prior disclosures, and maintained using an appropriate protocol to encourage the growth of soft tissue. Still another newly conceived application for the vacuum dome is as an aid in endoscopic or other minimally invasive surgery. In this application, a vacuum dome may be placed over a skin surface and used as an external retractor to lift up the surface integument to thereby create an optical cavity for subcutaneous endoscopic surgery. A pressure differential introduced within the dome may be used to separate the skin from the underlying tissue without interfering with either surgical access or viewing by the surgeon during the procedure. As such, this application for the vacuum dome provides distinctive advantage over several of the prior art approaches including the use of balloons to gently separate the skin from the underlying tissue. When in place, the balloon obviously interferes with surgical access and obscures surgical viewing. Applying a vacuum to the skin to encourage its separation may be done externally and thereby leave clear access in sight to the surgical point of contact.

[0025] In implementing any of the embodiments of these prior inventions, the inventor utilizes a dome which is positioned adjacent a skin surface and which requires an airtight seal between the dome and the skin surface. In several of these embodiments, a vacuum may be drawn within the dome as well. In utilizing this

construction, the inventor is aware of potential complications which can develop when an area of the body needs to be enclosed for prolonged periods of time within the dome having an airtight seal. For example, while a rim made of conforming or other soft materials may suffice for temporary use, a number of problems arise in the skin contact area when prolonged negative pressure application is necessary. The present invention includes in its various aspects various features which are intended to deal with these problems.

[0026] One such concern is for the management of the shear forces generated by the dynamic inward pull of the skin. As explained above, drawing a vacuum within the dome creates dynamic forces under the rim of the dome as the skin and other soft tissue is "pulled" up into the dome by the vacuum. Generally speaking, these forces place a shear force on the skin which has been found to be roughly equivalent to a normal force in that the skin blood flow decreased roughly linearly with the increase of shear forces. See the effect of shear forces externally applied to skin surface on underlying tissues by Zhang and Roberts, Journal of Biomedical Engineering, Vol. 15, No. 1, January 1993, pages 451-456. The effect of these shear forces may be dramatically minimized by providing an interface between the dome and the skin which allows inward displacement of the contact surface in response to the vacuum. There are numerous examples of structures which could achieve this desired inward displacement including a gel, an inflatable bladder, a bellows, a corrugated collapsible structure, or virtually any other mechanical/geometrical design which will allow substantially inward concentric movement of the contact surface area.

[0027] Still another problem encountered in applying a dome to a skin surface is the possibility for tissue damage at points of pressure concentration. It is well known from the literature on pressure sores that the body has numerous pressure points where bony prominences lack the thick layer of soft tissue padding needed to dissipate the pressure subjected to the overlying skin. These are the prominences where pressure sores tend to develop. Furthermore, with movement of the body parts, these pressure points are not static and fixed but have a tendency to shift from one cutaneous area to the other. To avoid creating points of pressure concentration at these shifting surfaces over bony prominences, it is important for the cushion under the dome to be able to constantly and evenly distribute the pressure on its underlying skin. This even distribution may be provided by a rim on the dome that has fluid-like properties. This cushion could be constructed with an air or fluid bladder, or any other type of membrane containing a gel-like fluid. Still other equivalent structures could be envisioned to achieve the same effect such as the use of a gel-like substance that can retain its contour and shape without a membrane layer boundary. This gel-like substance would approximate the hydraulic effect of a fluid-filled bladder.

[0028] A related problem to that of shifting points of pressure concentration is the overall contour of the body surface underlying the rim. This is especially the case as a wearer of the dome performs his routine daily activities. These routine daily activities would ordinarily shift the dome and would potentially cause the dome rim to contact other areas of the body not having the same contour as at the "at rest" orientation. For these reasons, the rim should be designed to constantly accommodate a potentially ever-changing contour for the underlying body surface. To achieve this, the rim should be flexible and have a surface with mechanical bending properties approximating those of the underlying body tissue. This may be achieved by using a cushion having the fluid-like properties as described above to accommodate pressure concentration caused by bony prominences.

[0029] Another significant consideration in utilizing a dome in the various inventions developed by the inventor herein is the requirement that an airtight seal be maintained to preserve minimal to small vacuum pressure differentials. Escaping air at the interface between the rim and the skin leads to loss of vacuum and necessitates frequent activation of a pressure pump. This is undesirable in that it is at best a nuisance. Loss of vacuum is untenable for a truly portable device which would require a portable pump and power supply. In any event, the integrity of the seal between the rim and the skin directly impacts on the useability and performance of the vacuum dome. Ideally, a cushion may be utilized under the rim and between it and the skin to provide an airtight seal without an excessive force being applied as excessive forces may themselves create tissue damage. A heightened seal integrity may be achieved through the use of a "sticky" material which may be placed under the cushion or surrounding the cushion so as to adhere and bond to the skin a surface which preserves the pressure integrity. This "sticky" aspect of the present invention may be achieved by utilizing a material for the cushion itself which has a sticky, gooey, gluey, or gummy surface property. Numerous materials including polymers such as silicone, hydrogels, and many other low durometer synthetic rubbers and gels have this inherent surface property. A sheet or layer of this "sticky" polymer or other material may be added as a skin surface contact sole to the undersurface of the cushion for the rim, with the cushion itself not exhibiting this "sticky" property. Still another alternative is a skin adhesive layer which can be painted, sprayed, or otherwise applied to the lower surface of the cushion intended to contact the patient's skin. Again, this would essentially form a "sole" for the rim cushion. Still another methodology may consist of applying a layer of adhesive by painting, spraying, or otherwise adhering a gluey or sticky surface directly to the skin itself. A "sticky" tape may be used as the sole or even a double-sided sticky skin tape can be provided to interface between the rim cushion and the skin. Those of ordinary skill in the art could conceive of other ways to achieve this "sticky" contact between the dome and the underlying skin in order to maintain the integrity of the seal. Furthermore, the combination of the relatively hard rim that can distribute the counter-pressures evenly along its width with the underlying cushion of

gel or fluid-filled bladder when combined with the adhesive "sticky" sole for maintaining the integrity of an airtight seal can be blurred and yet be covered by the inventor's inventive concepts. For example, these advantages may all be achieved through structure constructed out of the same material with a gradient of tackiness or durometer properties.

[0030] While the practical advantages and features of the present invention and method have been briefly described above, a greater understanding of the novel and unique features of the invention may be obtained by referring to the drawings and Detailed Description of the Preferred Embodiment which follow.

Brief Description of Drawings

[0031] Figure 1 is a front elevation view of the soft tissue enlargement apparatus, showing the breast augmentation embodiment; Figure 2 is a cross-sectional view of the breast enlargement embodiment taken in the plane of line 2-2 of Figure 1; Figure 3 is a cross-sectional schematic of a dome and soft tissue in the early stages of enlargement; Figure 4 is a cross-sectional schematic of a dome and soft tissue in the latter stages of enlargement; Figure 5 is an orthographic projection of the penile augmentation embodiment of the present invention; Figure 6 is a cross-sectional schematic of a fourth alternate embodiment wherein a flexible sheet which may be bonded to the soft tissue spans the rigid dome to prevent leakage between the dome and the skin; Figure 7 is a cross-sectional diagram of an alternate embodiment wherein a flexible rim gasket is used to distribute the forces along the rim; Figure 8 is a partial cross-sectional view of the dome and rim explaining the shear forces created at the rim; Figure 9 is a partial cross-sectional view of the dome and rim illustrating the inward displacement of the rim cushion in response to a vacuum within the dome; Figure 10 is a partial cross-sectional view of the rim and rim cushion partially deflected to accommodate a bony prominence; Figures 11A and 11B are cross-sectional views of the dome and rim with the rim cushions deflected to accommodate changes in the contour of the body surface; Figure 12 is a partial cross-sectional view of the dome and rim with rim cushion, with a layer of sticky sole interfaced between the rim cushion and skin; Figures 13A and 13B depict the application of the dome to an amputated stump of either a fresh amputation or an amputation having deficient soft tissue; Figure 14 depicts the vacuum dome applied over a skin flap and adapted for endoscopic surgery to assist in separating a skin flap from the underlying musculature; Figure 15 is a prospective view of a breast enlargement bra utilizing vacuum domes with a surrounding adhesive-coated bra; Figure 16 is a partial cross-sectional view of the bra depicted in Figure 15 and detailing the vacuum dome, cushioned rim, and surrounding adhesive-coated strap arrangement; and Figures 17A, 17B, 17C, and 17D depict various alternatives for mechanical rim cushions.

Detailed Description

[0032] One embodiment of the soft tissue enlargement apparatus 10 is generally comprised of a dome 12 having a rim 14 and a vacuum pump assembly 16 for creating a vacuum within the dome. Although the vacuum pump assembly 16 may be a separate hand-held pump in one variant embodiment, in the preferred embodiment the vacuum pump assembly 16 is a self-contained vacuum pump 20 with an independent power source 22, pressure sensor 24, and servomechanism 26 for driving, regulating and controlling the vacuum pump 20.

[0033] Regulation of the vacuum within the dome is essential to prevent contusions caused by rupturing capillaries adjacent the surface of the skin. Medical data suggest that these contusions will not occur if vacuum within the dome is maintained at less than 20 mmHg. Thus, the vacuum pump 20 must be regulated to control the vacuum within the dome to within this limit. In addition, skin ulceration can occur if excessive contact pressures are applied thereto. Medical data suggest that a contact pressure less than 20 mmHg may be applied indefinitely without such ulceration. However, contusions may occur due to positive contact pressures upon the skin at pressures above this ulceration limit. The preferred embodiment of the present invention was developed with these limits in mind and will not apply a vacuum greater than 20 mmHg or constant contact pressure greater than 20 mmHg.

[0034] Several forces are developed within the dome and about the rim as a result of evacuating air from the dome. A suction or tensile force F_s is developed within the dome 12 equal to the vacuum pressure P_1 multiplied by the enclosed tissue surface area 30, A_s . The vector sum of the tensile force upon the tissue surface area 30 may be called the normal force F_1 and is equal to the vacuum pressure multiplied by the normal area 32, A_1 of the dome opening, i.e., the projected area bounded by the periphery 33, or $F_1 = P_1 A_1$. An opposing force F_2 is imposed on the user by the rim 14 to balance the normal force F_1 and is equal but opposite to the normal force. The contact pressure P_2 of the rim 14 against the user is equal to this opposing force F_2 divided by the annular rim surface area 34, A_2 , i.e., $P_2 = F_2 / A_2$ or $F_2 = P_2 A_2$. As the magnitude of the opposing force is equal to the magnitude of the normal force, $F_1 = F_2$ and $P_1 A_1 = P_2 A_2$. Therefore, if the rim surface area 34, A_2 is configured to be greater than or equal to the normal area 32, A_1 at the dome opening, then the contact pressure against the patient's skin will not exceed the magnitude of the vacuum within the dome 12, i.e., $P_2 = P_1$. Similarly, the rim surface area 34, A_2 may be sized with respect to the normal area 32, A_1 so that the contact pressure P_2 is maintained below 20 mmHg when the vacuum pressure P_1 within the dome is maintained at less than 20 mmHg. Likewise, if the vacuum pressure is cycled, different area ratios may be used to optimize the therapeutic effects while

minimizing the potential for damage to the soft tissue within the dome or beneath the rim.

[0035] As the soft tissue enlarges, the rate of enlargement increases due to a beneficial physical phenomenon. If the tissue only slightly protrudes into the dome as shown in Figure 3 and as is typically the initial condition, then the surface area 30 under the dome is only slightly larger than the normal area 32 at the dome opening. Therefore, the vacuum pressure P_1 acts on a surface area 30 which approaches the minimal value of the normal area. As enlargement occurs, more tissue protrudes into the dome 12 as shown in Figure 4 thereby providing more surface area 30 under the dome. Because the surface area 30 under the dome is larger, the area over which the vacuum pressure acts is larger. For a given pressure, the enlargement of the soft tissue is a function of the surface area. Therefore, the total rate of enlargement of the soft tissue increases as treatment continues because the surface area under the dome is ever increasing. In other words, with more tissue under the dome the tensile force F_s is greater ($F_s = PA_s$) and the breast grows larger faster. This however has no effect on the opposing force, or for that matter the normal force, as the tensile force F_s is a vector which must always sum into the normal force. In still other words, a unit of surface area enlarges at a constant rate for any given pressure, but as the soft tissue surface area under the dome increases, there are more units of surface area increasing at the constant rate. Therefore, the total rate of enlargement increases as treatment continues even though the vacuum pressure is not increased.

[0036] One specific embodiment includes a dome 12 configured to fit over a human breast as shown in Figures 1 and 2. This embodiment includes a rim 14 having a surface area 34 approximately equal to the normal area 32 of the dome opening thereby preventing medical complications to the soft tissue as long as the pressure is properly regulated within the dome 12. However, alternate embodiments having a rim 14 with a surface area 34 equal to or less than the normal area 32 of the dome opening may be used depending upon the amplitude of the vacuum pressure used and depending upon whether the vacuum pressure is constant or varied. The pressure reducing means 16 is located underneath the patient's breast, so that the apparatus 10 may be hidden under loose-fitting clothes. As with the general embodiment, the vacuum pump assembly 16 of this embodiment is preferably comprised of a vacuum pump 20 with a power source 22, a pressure sensor 24 and servomechanism 26 to drive and control the vacuum pump and to regulate the pressure within the dome 12.

[0037] As shown in Figure 1, this specific embodiment may take the form of a bra 40 having two domes 12 spaced by a hinge 42. Straps 44 may be attached to the bra 40 to retain the bra 40 in place. A gasket 46 may also be included about the rim 14 to improve the patient's comfort and enhance the seal about the rim. In the preferred embodiment, this gasket 46 may be a silicone gel cushion or other soft, conforming

[0041] More particularly, as shown in Figure 8, and as is explained in greater detail in the Biomedical Engineering article referenced above, there are dynamic forces which act on the skin surface under the rim 14 of dome 12. They are illustrated in Figure 8 as F_{cp} as the counterforce generated by the static effect of the pressure as the vacuum is generated inside the dome 12 which forces it inward towards the skin surface. F_{dp} is the counterforce generated by the dynamic inward pull on the skin surface as it is stretched inwardly by the vacuum effect. This is the shearing force which places the skin surface in tension. F_r is the resultant force, or vector sum of these two forces, exerted on the skin surface by the vacuum within dome 12 and rim 14. At the inner lip of the dome (.A), the resultant force F_r is much greater than the static effect of the vacuum alone. This added effect of the dynamic shear forces and the static pressure force tends to damage the skin just under the inner lip. This was observed by the inventor during limited human trials. For the vacuum dome to be successfully used in cosmetic applications, or indeed for that matter in order to avoid any injury to the patient caused by the vacuum dome, it is desired that this resultant force be accommodated without injury to the patient.

[0042] As shown in Figure 9, the dome 12 is supported at a modified rim 14 with an underlying gasket (hereinafter referred to as "cushion") 46 which is sufficiently flexible to allow inward displacement as the skin surface is drawn into the dome 12 by the effect of the vacuum therewithin. As the skin surface is relatively free to "shift" with respect to the rim 14 by the deflexion of cushion 46, the shear force is distributed along the entirety of the lower surface of the rim cushion 46 and is not concentrated at a single point A as is illustrated in Figure 8 with a rigid rim 14. In other words, points A, B, and C on the rim cushion 46 prior to pulling a vacuum within dome 12 are shifted to points A', B', and C' as the vacuum is generated and the rim cushion 46 deflects. By distributing this shear force across the lower surface of the rim cushion 46, and indeed even beyond as additional peripheral skin is recruited, potential skin damage attributable to this shearing action is minimized.

[0043] Desirable attributes for the rim cushion 46 in order to achieve this concentric shifting along the circumferential rim, in the embodiment depicted in Figures 8 and 9, includes a height dimension which should accommodate a sufficient amount of deflexion desirable to dissipate the shear force. The inventor has found that a height of approximately 2 cm or more in a pressure dome sized to accommodate a typical female breast is adequate. The cushion 46 should have inherent lateral flexibility to allow for repeated bending, deflecting, and rotation. Also, the cushion 46 should be relatively soft, especially along its lower surface, with reduced potential for the formation of any firm or hard skin surface contact area.

[0044] As explained, the embodiment shown in Figure 9 may be comprised of a gel, inflatable bladder, etc. However, the inventor's concept includes any kind of a

mechanical arrangement which would permit relatively uniform concentric displacement. Alternative examples are shown in Figures 17A-D and include a foam 70 formed from a polyurethane or other similar substance, a ribbed or "swiss cheese" like construction where various orifices 72 are formed within a semi-rigid or flexible rim cushion 46. Also as shown in Figure 17D, a bellows 74 or accordion-like construction may be provided which could freely move and accommodate a reduced diameter upon deflexion thereof in response to the pulling of a vacuum within the dome. Other mechanical arrangements which would achieve this desired flexure or displacement would be apparent to those of ordinary skill in the art and are included within the scope of the inventor's concept.

[0045] As shown in Figure 10, still another physical attribute desirably accommodated by the vacuum dome and rim includes potential points of pressure concentration caused by a rib or other bony prominence 76 underlying the skin surface. As depicted therein, the rim cushion 46 underlying rim 14 should be sufficiently flexible to avoid creating a point of pressure concentration which could contribute to causing pressure sores or the like. This flexibility may be achieved for the use of a fluid-like cushion, an air-filled fluid bladder, a gel-like fluid, or such other construction and materials as would be effective to distribute the pressure substantially uniformly across the skin surface underlying the rim cushion 46.

[0046] As shown in Figures 11A-B, the fluid-like cushion 46 described above, in some applications, should also accommodate an ever-changing contour of the skin surface as the user experiences his activities of daily living. This helps to avoid any potential vacuum loss from within dome 12 which would require reestablishing the vacuum. This helps to ensure reliable application of the vacuum to the intended skin surface without undo involvement with a pump. This ensures reliable results and inconvenience to the patient.

[0047] As shown in Figure 12, the inventor has also found it desirable to seal the rim cushion 46 to the skin surface through the use of a "sticky" sole interfaced between the rim cushion 46 and the skin surface. This "sticky" sole may be comprised of a number of alternative constructions. For example, the cushion 46 may itself be made of materials which exhibit a sufficiently "sticky" surface property so as to in and of itself provide this "sticky" function. Numerous polymers such as silicone, hydrogels, and many other low durometer synthetic rubbers and gels have this inherent surface property. Alternatively, another substance may be applied to the cushion 46, the underlying skin surface, or any combination thereof in order to achieve this "sticky" seal to ensure that the vacuum within dome 12 is reliably maintained as best as is feasible under the circumstances. This "sticky" sole 78 could also be a sheet or layer of an adhesive material, an adhesive layer may be applied to either the skin surface or rim cushion 46, a tape could be applied between the rim cushion 46 and skin surface, or

[0051] There are various changes and modifications which may be made to the invention as would be apparent to those skilled in the art. However, these changes or modifications are included in the teaching of the disclosure and it is intended that the invention be limited only by the scope of the claims appended hereto.

Claims

[c1]

An apparatus for enhancing living tissue comprising:

a vessel having an open end and adapted to encompass the tissue to be enhanced;

a source of vacuum connected to said vessel; and

a flexible mass affixed to the open end of said vessel to absorb the pressure exerted by said vacuum, thereby acting as a seal and force diffuser between the vessel and the tissue adjacent the periphery of said vessel.

[c2]

The apparatus in accordance with claim 1, wherein said vessel has a shape generally conforming to the shape of the tissue to be enhanced.

[c3]

The apparatus in accordance with claim 1, wherein said vessel has a volume greater than the volume of tissue to be enhanced.

[c4]

The apparatus in accordance with claim 1, wherein said vessel has a shape which is varied to control the shape of the tissue enhanced.

[c5]

The apparatus in accordance with claim 1, wherein said vessel is dome-shaped having a periphery to surround the tissue to be enhanced.

[c6]

The apparatus in accordance with claim 1, wherein said vessel has an opening separate from said open end for connection to said source of vacuum.

[c7]

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